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## INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

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(60) Parent Application or Grant INTA-MEDICS LTD. [/], (). MICHAELI, David [/]; (). MICHAELI, David [/], ().		
(54) Title: NONINVASIVE MONITORING OF INTRACRANIAL PRESSURE (54) Titre: SURVEILLANCE NON INVASIVE DE LA PRESSION INTRACRANIEUNE		
(57) Abstract <p>A noninvasive method of monitoring the intracranial pressure (ICP) of a patient. At least one waveform representative of a pulsation of an anatomical feature of the patient's head is obtained, preferably by integrating ultrasound reflection traces in a time gate corresponding to reflections from the feature. The preferred anatomical feature is the third cerebral ventricle. A quantitative measure of ICP is inferred from two or more diagnostic features, such as diagnostic times, associated with the waveform. Alternatively, a qualitative measure of ICP is obtained from the shape of the respiratory wave imposed on the train of waveforms by the patient's breathing.</p>		
(57) Abrégé <p>L'invention concerne une méthode permettant de surveiller de manière non invasive la pression intracrânienne d'un patient. On obtient au moins un oscillogramme représentant une pulsation d'une caractéristique anatomique de la tête du patient, de préférence en intégrant des traces de réflexion d'ultrasons dans une porte temporelle correspondant à des réflexions de ladite caractéristique. De préférence, ladite caractéristique anatomique est le troisième ventricule cérébral. On infère une mesure quantitative de la pression intracrânienne à partir d'au moins deux caractéristiques de diagnostic, telles que des heures de diagnostic, associées à l'oscillogramme. Dans une variante, on obtient une mesure qualitative de la pression intracrânienne à partir de la forme de la courbe respiratoire imposée au train d'ondes par la respiration du patient.</p>		

PCT

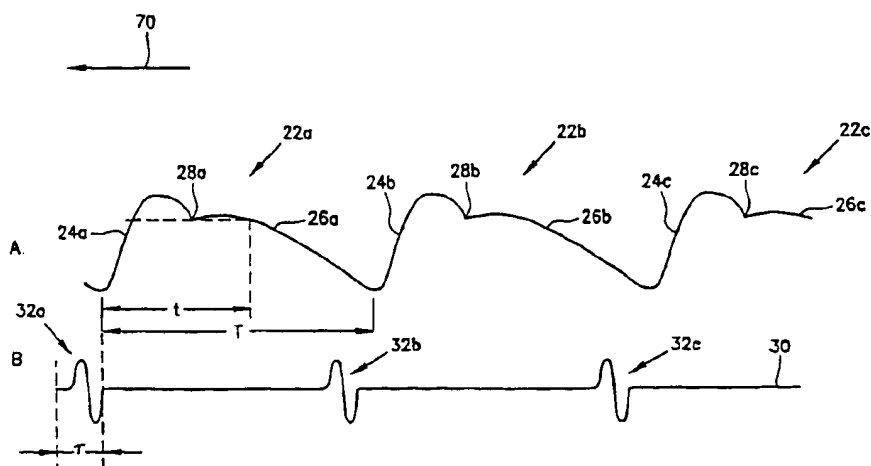
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(21) International Application Number: PCT/IB00/00595 (22) International Filing Date: 9 May 2000 (09.05.00) (30) Priority Data: 09/307,568 10 May 1999 (10.05.99) US (71) Applicant (for all designated States except US): INTA-MEDICS LTD. [IL/IL]; South Industrial Zone, Ashkelon, P.O. Box 7284, 78172 Ashkelon (IL). (72) Inventor; and (75) Inventor/Applicant (for US only): MICHAELI, David [IL/IL]; Marheshvan 7/6, Ashkelon (IL).		(81) Designated States: AE, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CR, CU, CZ, DE, DK, DM, EE, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TR, TT, TZ, UA, UG, US, UZ, VN, YU, ZA, ZW, ARIPO patent (GH, GM, KE, LS, MW, SD, SL, SZ, TZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GW, ML, MR, NE, SN, TD, TG).  Published Without international search report and to be republished upon receipt of that report.

(54) Title: NONINVASIVE MONITORING OF INTRACRANIAL PRESSURE



(57) Abstract

A noninvasive method of monitoring the intracranial pressure (ICP) of a patient. At least one waveform representative of a pulsation of an anatomical feature of the patient's head is obtained, preferably by integrating ultrasound reflection traces in a time gate corresponding to reflections from the feature. The preferred anatomical feature is the third cerebral ventricle. A quantitative measure of ICP is inferred from two or more diagnostic features, such as diagnostic times, associated with the waveform. Alternatively, a qualitative measure of ICP is obtained from the shape of the respiratory wave imposed on the train of waveforms by the patient's breathing.

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Description

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5 Furthermore, the threaded fitting may penetrate the patient's brain, causing damage to the patient's brain.

10 In both of the latter two invasive methods, the catheter must be removed after five days. Therefore, these methods can not be used for long term (several months) monitoring of ICP of patients in comas.

15 In a fourth invasive method, a fiber optic device, with a sensor at the tip of a fiber optic cable, is inserted in the patient's cerebral tissue, in the patient's subdural space, or in the patient's intraventricular epidural space. If a blood clot forms on the sensor, or if the fiber optic cable  
20 bends too sharply or breaks, the device may give a spuriously high pressure reading.

In short, the prior art invasive methods of measuring ICP are unreliable, may lead to  
25 infection, and can not be used for more than five consecutive days.

There are additional reasons why it would be advantageous to have a non-invasive  
30 method of monitoring ICP.

The standard quantitative measure of the severity of coma is the Glasgow Coma Scale.  
See Mark S. Greenberg (ed.), *Handbook of Neurosurgery*, 4<sup>th</sup> edition (1988), vol. 2 p. 553. The  
35 score value of the scale ranges from 15 for a normal individual to 3 for a patient in deep coma. The prior art protocol is to start ICP monitoring if the score is 8 or less. It would be useful to monitor ICP of patients with scores higher than 8.

40 It also would be useful to monitor the ICP of healthy individuals under severe environmental stress, for example, astronauts, divers and submariners.

45 Yost et al., in US Patent No. 5,617,873, purport to describe an indirect, noninvasive method of monitoring ICP. Two changes in CSF volume are induced, and the associated changes in ICP are measured. The absolute value of ICP is inferred from these measurements. Although



5 the methods they teach for measuring the changes in ICP in fact are noninvasive, their methods of *inducing* changes in CSF volume are necessarily invasive, despite their claims to the contrary.

10 Transcranial Doppler monitoring is a noninvasive technique that provides only qualitative indications of variations in ICP, not the quantitative measurements provided by the prior art invasive methods.

15 Michaeli, in US Patent No. 5,840,018, which is incorporated by reference for all purposes as if fully set forth herein, teaches a noninvasive method for diagnosis of migraines, based on ultrasound measurements of the diameters of cranial blood vessels. Ultrasound reflection traces are integrated within a preselected gate to provide samples of an Echo Pulsogram (EPG) signal.  
20 The timing of the gate is selected to correspond to the depth within the cranium of the target blood vessel. The time lag between start systole, as indicated by an Electrocardiograph (ECG) signal, and the start of contraction of the target blood vessel, as compared to the normal time lag  
25 of  $211 \pm 6$  milliseconds, is diagnostic of migraines.

#### SUMMARY OF THE INVENTION

30 According to the present invention there is provided a method for measuring intracranial pressure in a head of a patient, the head including a forehead and a bridge of a nose, including the steps of: (a) measuring, entirely from outside the head of the patient, at least one waveform  
35 representative of a pulsation of an anatomical feature in the head of the patient; (b) identifying a plurality of diagnostic features associated with the at least one waveform; and (c) inferring the intracranial pressure from the plurality of diagnostic features.

40 The shapes of anatomical features of a patient's skull, such as the cerebral ventricles, change in synchrony with the patient's heartbeat. The present invention is based on an empirical relationship between these shape pulsations and ICP. According to the present invention, a  
45 waveform, or a series of waveforms, representative of the pulsation of the shape of one of these anatomical features, is measured noninvasively, and the empirical relationship is used to infer

5 ICP. The preferred anatomical feature is the third ventricle. The preferred modality for  
measuring the waveform is ultrasound. The preferred waveform is obtained by integrating  
10 ultrasound reflection traces within a predetermined gate corresponding to a reflection from the  
anatomical feature.

According to a first embodiment of the present invention, a ratio of diagnostic times that  
15 characterize the waveform is determined. An empirical quadratic relationship between this ratio  
and ICP as measured by a prior art invasive method is used to infer ICP quantitatively.

20 According to a second embodiment of the present invention, several successive  
waveforms are received, over the course of at least one respiratory cycle. The shape of the  
corresponding respiratory wave, as reflected in the successive waveforms, is related qualitatively  
to the ICP.

#### 25 BRIEF DESCRIPTION OF THE DRAWINGS

The invention is herein described, by way of example only, with reference to the  
30 accompanying drawings, wherein:

FIG. 1A is a sketch of EPG waveforms over the course of several cardiac cycles;

FIG. 1B is a sketch of an ECG trace synchronous with the waveforms of FIG 1A;

35 FIG. 2 shows  $\rho$  as a function of  $t/T$ ;

FIGS. 3A and 3B are sketches of waveform trains modulated by a patient's breathing.

#### 40 DESCRIPTION OF THE PREFERRED EMBODIMENTS

The present invention is of a noninvasive method of quantitative and qualitative  
45 monitoring of ICP.

5           The principles and operation of noninvasive monitoring of ICP according to the present invention may be better understood with reference to the drawings and the accompanying description.

10           As used herein, a waveform is said to be representative of a pulsation of an anatomic feature if the shape of the waveform, as a function of time, is isomorphic with the shape of the anatomical feature, as a function of time, up to a sign. For example, the geometric dimensions  
15 of a patient's third ventricle increase and decrease in synchrony with the change in the patient's blood pressure over the course of the patient's cardiac cycle. A waveform whose amplitude increases as a corresponding dimension of the third ventricle increases, and whose amplitude  
20 decreases as that dimension of the third ventricle decreases, is said to be representative of the pulsation of the third ventricle over the course of the cardiac cycle. This isomorphic representation is up to a sign, so a waveform whose amplitude decreases as a corresponding  
25 dimension of the third ventricle increases, and whose amplitude increases as a corresponding dimension of the third ventricle decreases, also is said to be representative of the pulsation of the third ventricle over the course of the cardiac cycle.

30           Although the scope of the present invention includes the measurement of waveforms representative of any anatomical feature of a patient's head, including, for example, the frontal cornum, the temporal cornum and the occipital cornum of the first and second ventricles, as well  
35 as the fourth ventricle, the preferred anatomical feature is the third ventricle. Again, although the scope of the present invention includes any noninvasive modality for measuring waveforms representative of pulsations of the target anatomical feature, the preferred modality is ultrasound. An ultrasound transducer is placed in contact with the patient's forehead. Pulses of ultrasound  
40 energy are introduced to the patient's head, in the sagittal direction, using the transducer. These pulses are partly reflected from anatomical features, including the target anatomical feature, that lie in their propagation paths. The reflections propagate back to the transducer, where they are  
45 converted into reflection traces. The desired waveforms are obtained by integrating each of the traces within a predefined gate, as taught in US Patent No. 5,840,018. Each resulting integration value is a sample of an EPG waveform.

5 Referring now to the drawings, Figure 1A shows two EPG waveforms 22a and 22b and  
a part of a third waveform 22c thus obtained, as a function of time. Each waveform 22 includes  
a monotonically rising portion 24 and a falling portion 26, with falling portion 26 including a  
10 venous output notch 28. For reference, Figure 1B shows an ECG trace 30, synchronized with  
EPG waveforms 22, that includes several ECG pulses 32. The start of each waveform 22 is  
coincident with the end of the corresponding ECG pulse 32. The direction of movement is  
indicated by an arrow 70. The start of each EPG waveform 22 is delayed relative to the start of  
15 the corresponding ECG pulse 32 by a delay  $\tau$ .

20 It has been determined empirically that the best location for the ultrasound transducer on  
the forehead of the patient is from 2.5 centimeters to 6 centimeters above the bridge of the  
patient's nose.

25 The features of waveforms 22 that are diagnostic of ICP are two diagnostic times  $T$  and  
 $t$ , shown in Figure 1A with reference to waveform 22a. Diagnostic time  $T$  is the duration of  
waveform 22, i.e., the duration of one cardiac cycle. Diagnostic time  $t$  is the length of time from  
the start of waveform 22 until the time, subsequent to the time of venous output notch 28, at  
30 which the amplitude of falling portion 26 returns to the amplitude of waveform 22 at the time  
of venous output notch 28. Because time  $t$  is shorter than the full duration of one waveform 22,  
time  $t$  is referred to herein as a "subduration".

35 By calibrating with invasive measures of ICP, it has been determined that the following  
equation describes ICP in terms of the ratio  $t/T$  with a 96% correlation:

$$40 \quad \text{ICP} = \rho(t/T) - B$$

45 The constant  $B$  is 9 mm H<sub>2</sub>O. For  $t/T$  less than about 0.3,  $\rho$  also is a constant, 373 mm H<sub>2</sub>O. For  
 $t/T$  greater than about 0.5,  $\rho$  itself varies quadratically with  $t/T$ , as shown in Figure 2. Note that  
the units of the ordinate in Figure 2 are mm H<sub>2</sub>O.

5 As the patient breathes, the train of waveforms 22 shown in part by Figure 1A may be modulated by that breathing. If the ICP is less than 15 mm Hg, the overall shape of the train of waveforms 22 is flat, as in Figure 1A, over many cardiac cycles. It is known from invasive  
10 studies that if the ICP is greater than about 20 mm Hg, the train of waveforms 22 is modulated by a respiratory wave (Greenberg, *op. cit.*, pp. 710-711). If the ICP is in the range of 20 to 40 mm Hg, the respiratory wave is in the form of a  $\beta$ -wave 40, as shown in Figure 3A.  $\beta$ -wave 40 includes cycles 42 of roughly equal periodicity that tend to have sharp peaks 44 and smooth  
15 troughs 46. Diagnostic features 42, 44 and 46 of  $\beta$ -wave 40 define the shape of  $\beta$ -wave 40 as roughly sinusoidal. If the ICP is in the range of 40 to 60 mm Hg, the respiratory wave is in the form of a plateau wave 50, as shown in Figure 3B. The shape of plateau wave 50 is defined by a series of cycles 52, with each cycle 52 starting with a sharp rise 54 to a sharp peak 56, declining  
20 to a plateau 58, and then declining further to a baseline 60. Monitoring successive waveforms 22 over several respiratory cycles to observe the shape of the respiratory wave provides a qualitative indication of ICP.

25 While the invention has been described with respect to a limited number of embodiments, it will be appreciated that many variations, modifications and other applications of the invention may be made.

Claims

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WHAT IS CLAIMED IS:

10 1. A method for measuring intracranial pressure in a head of a patient, the head including a forehead and a bridge of a nose, comprising the steps of:

- 15 (a) measuring, entirely from outside the head of the patient, at least one waveform representative of a pulsation of a ventricle in the head of the patient;
- (b) identifying a plurality of diagnostic features associated with said at least one waveform; and
- (c) inferring the intracranial pressure from said plurality of diagnostic features.

20 2. The method of claim 1, wherein said ventricle is a third ventricle.

25 3. The method of claim 1, wherein said measuring of said waveform is effected by steps including repeatedly receiving ultrasound echoes from said anatomical feature, said echoes defining said waveform.

30 4. The method of claim 3, wherein said receiving of said ultrasound echoes is effected by steps including:

- (i) placing an ultrasound transducer in contact with the head of the patient;
- 35 (ii) repeatedly introducing pulses of ultrasound energy into the head of the patient, using said transducer; and
- (iii) for each of said pulses, receiving a reflection trace of said pulse.

40 5. The method of claim 4, wherein said waveform is obtained from said reflection traces by integrating each of said reflection traces within a predetermined gate, said integration of said each reflection trace providing a sample of said waveform.

45 6. The method of claim 4, wherein said receiving of said reflection traces is effected using said transducer.

5           7.     The method of claim 6, wherein said ultrasound transducer is placed in contact with the forehead of the patient, between about 2.5 centimeters and about 6 centimeters above the bridge of the nose.

10           8.     The method of claim 1, wherein said plurality of diagnostic features includes a plurality of diagnostic times.

15           9.     The method of claim 8, wherein said plurality of diagnostic times includes a duration and a subduration.

20           10.    The method of claim 9, wherein the intracranial pressure is inferred from a ratio of said subduration to said duration.

25           11.    The method of claim 10, wherein the intracranial pressure is inferred from a linear function of said ratio.

30           12.    The method of claim 1, wherein said measuring of said at least one waveform is effected for a sufficiently long time to include at least one respiratory wave.

35           13.    The method of claim 12, wherein said plurality of diagnostic features defines a shape of said at least one respiratory wave.

40           14.    A method for measuring intracranial pressure in a head of a patient, the head including a forehead and a bridge of a nose, comprising the steps of:

          (a)     measuring, entirely from outside the head of the patient, at least one waveform representative of a pulsation of an anatomical feature in the head of the patient by:

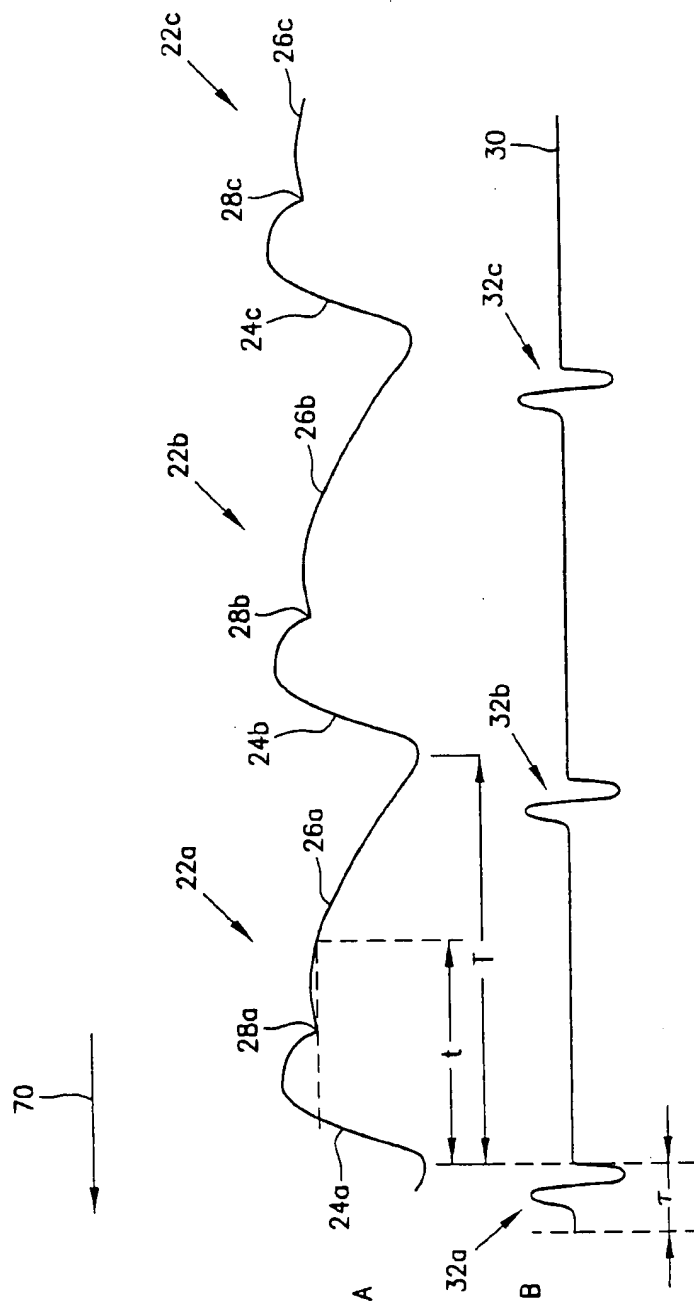
45           (i)    placing an ultrasound transducer in contact with the forehead of the patient, between about 2.5 centimeters and about 6 centimeters above the bridge of the nose,



- 5 (ii) repeatedly introducing pulses of ultrasound energy into the head of the patient, using said transducer, and
- 10 (iii) for each of said pulses, receiving a reflection trace of said pulse, using said transducer, said reflection traces defining said waveform;
- (b) identifying a plurality of diagnostic features associated with said at least one waveform; and
- 15 (c) inferring the intracranial pressure from said plurality of diagnostic features.
15. A method for measuring intracranial pressure in a head of a patient, comprising the steps of:
- 20 (a) measuring, entirely from outside the head of the patient, at least one waveform representative of a pulsation of an anatomical feature in the head of the patient;
- (b) identifying a duration and a subduration associated with said at least one waveform; and
- 25 (c) inferring the intracranial pressure from said duration and said subduration.
16. A method for measuring intracranial pressure in a head of a patient, comprising the steps of:
- 30 (a) measuring, entirely from outside the head of the patient, for a sufficiently long time to include at least one respiratory wave, at least one EPG waveform representative of a pulsation of an anatomical feature in the head of the patient;
- 35 (b) identifying a plurality of diagnostic features, associated with said at least one waveform, that define a shape of said respiratory wave; and
- 40 (c) inferring the intracranial pressure from said plurality of diagnostic features.
17. A method for measuring intracranial pressure in a head of a patient, comprising the steps of:
- 45 (a) measuring, entirely from outside the head of the patient, at least one EPG waveform representative of a pulsation of an anatomical feature in the head of the patient;

- 5 (b) identifying a plurality of diagnostic features associated with said at least one  
waveform; and
- (c) inferring the intracranial pressure from said plurality of diagnostic features.
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Fig. 1

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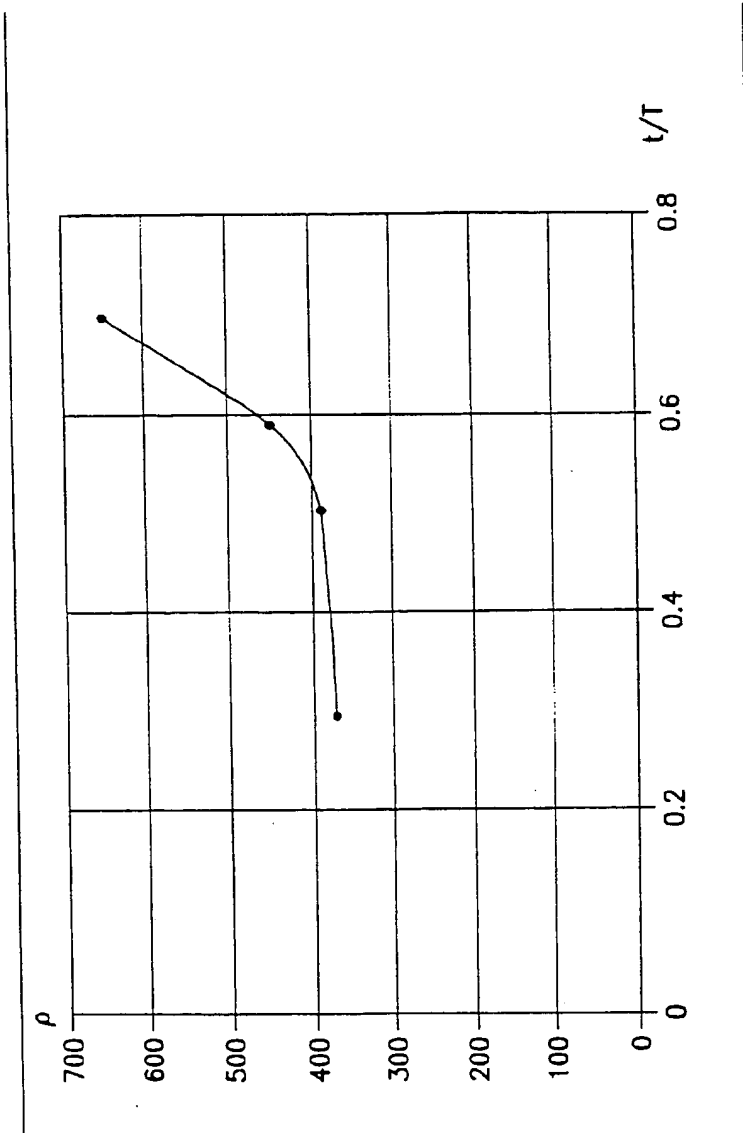


Fig. 2

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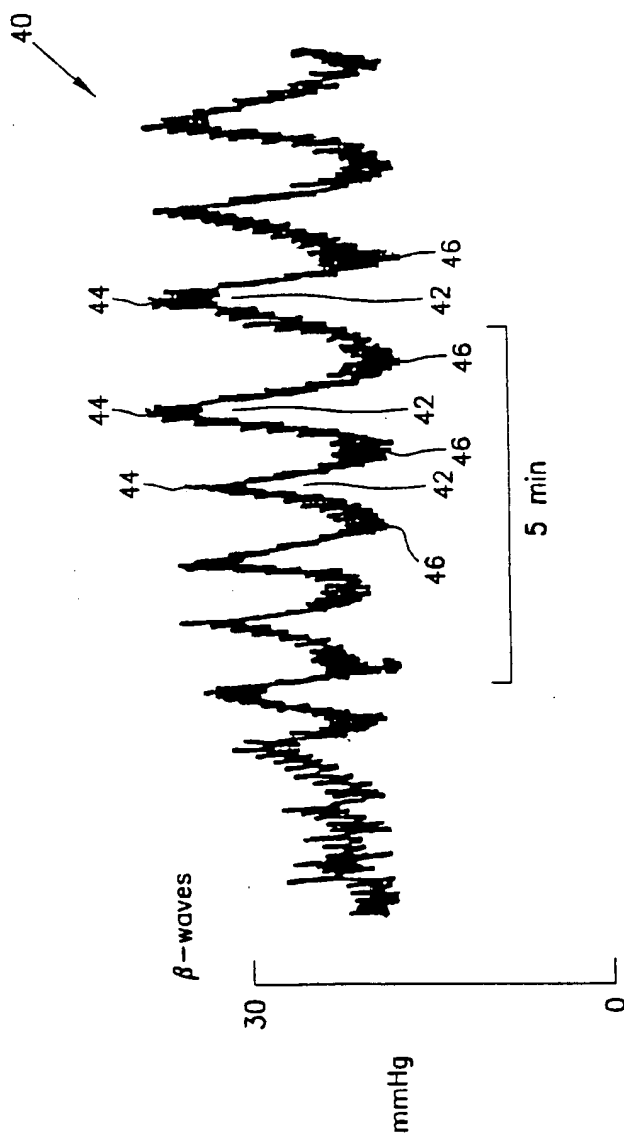


Fig. 3A

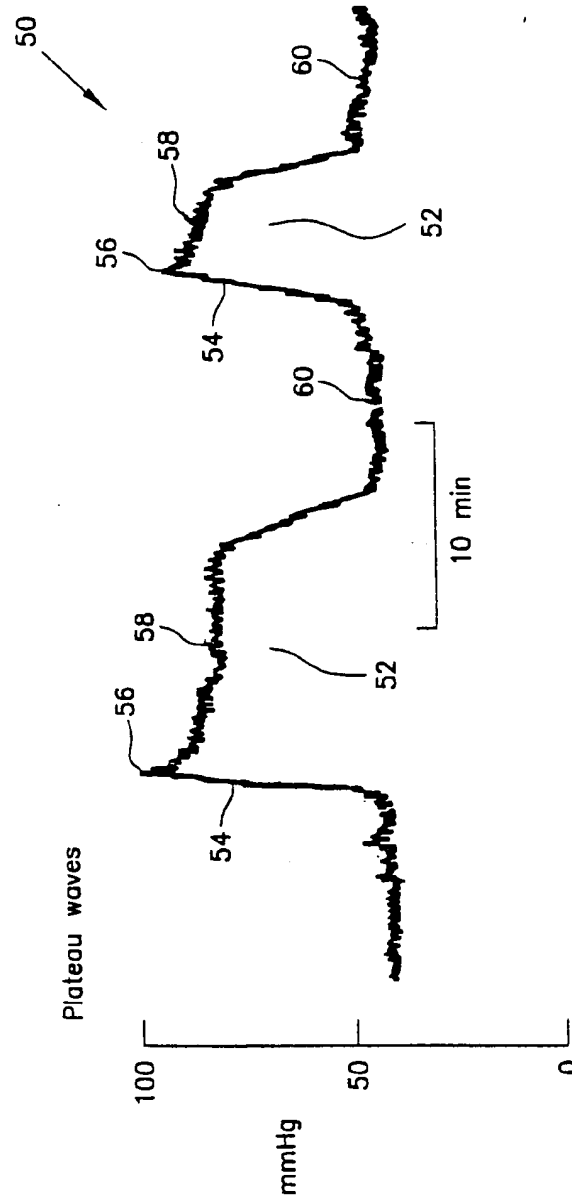


Fig. 3B